

Real-Time Anomaly Detection on Wearables using Edge AI

Aswathnarayan Muthukrishnan Kirubakaran
California, USA
0009-0006-6652-2663

Akash Kumar Agarwal
California, USA
0009-0006-7872-3446

Lokesh Butra
North Carolina, USA
0009-0009-0286-9635

Sumit Saha
California, USA
0009-0009-5888-3110

Suhas Malempati
South Carolina, USA
0009-0009-3855-0423

Abhirup Mazumder
Texas, USA
0009-0008-4811-8477

Abstract—Wearable devices are increasingly used for continuous monitoring of physiological signals and human movement; however, existing systems often rely on cloud-dependent analytics, single-sensor thresholds, or delayed inference workflows that limit their usefulness during real-time emergencies. This paper introduces EdgeSense Health, an edge-native architecture for low-latency detection of physiological and mobility anomalies using multi-modal sensor fusion. The framework integrates synchronized accelerometer, gyroscope, ECG, PPG, SpO₂, and skin-temperature streams with a lightweight deep learning pipeline combining convolutional feature extraction, Transformer-based temporal modeling, and variational autoencoder-driven anomaly scoring. To support real-time operation, inference executes directly on wearable-class microcontrollers or embedded processors, avoiding cloud latency and strengthening privacy by minimizing data egress. A prototype evaluation involving controlled physiological stressors, tremor events, gait perturbations, falls, and hypoxia simulations demonstrates that EdgeSense Health achieves detection latencies under 20 ms and maintains high accuracy across anomaly categories. This architecture provides a practical and scalable foundation for next-generation wearable health monitoring and human-state awareness applications.

Index Terms—Edge AI, sensor fusion, anomaly detection, multi-modal wearables, physiological monitoring.

I. INTRODUCTION

Wearable sensing platforms have evolved significantly over the past decade, transitioning from simple activity-tracking devices into powerful multi-modal health assessment tools capable of analyzing complex physiological and biomechanical patterns [1]. Modern wearables incorporate optical, electrical, inertial, and thermal sensing capabilities, making continuous monitoring of cardiovascular, respiratory, and movement-related indicators possible outside clinical settings [2], [3]. These signals often contain early markers of adverse physiological events, including arrhythmias, hypoxic episodes, acute respiratory irregularities, tremor intensification, gait instability, and sudden collapse [4], [5].

Despite this potential, current commercial systems exhibit several architectural limitations [6]. Many rely on *cloud-centric* processing pipelines in which raw or lightly processed sensor data are streamed to remote servers for inference [7]. Such designs impose non-deterministic latency, degrade performance under intermittent connectivity, increase cost of

data transmission, and raise privacy concerns due to the continuous movement of raw physiological data. Simultaneously, threshold-based on-device algorithms lack the sensitivity and adaptability required for early anomaly detection, particularly under noisy real-world conditions [8].

Edge-native AI provides an attractive alternative by executing inference directly on the wearable device or a nearby gateway [9]. However, this poses technical challenges: multi-modal physiological and inertial streams differ in frequency, noise characteristics, and sampling artifact behavior, and must be synchronized precisely under strict memory and computational constraints. Temporal dependencies especially those spanning tens of seconds are difficult to model on low-power microcontrollers. Additionally, personalization is crucial; physiological baselines vary significantly across individuals and contexts [10].

This paper proposes EdgeSense Health, a unified multi-modal edge-native anomaly detection architecture that addresses these challenges. The system integrates synchronized sensor fusion, hybrid deep neural modeling, and personalized anomaly scoring while operating within the severe computational limits of embedded hardware. EdgeSense Health demonstrates that clinically meaningful physiological and mobility anomalies can be detected reliably and consistently without relying on cloud computation, making the approach suitable for continuous monitoring in real-world environments [11].

II. RELATED WORK

A. Physiological Signal Analysis

Classical physiological monitoring approaches rely heavily on handcrafted features derived from ECG, PPG, and respiration signals. While effective for certain tasks, these systems often underperform under motion-induced noise or sensor misalignment. Deep learning-based approaches have shown improved robustness by learning morphological and temporal dependencies directly from data [12]; however, they typically require inference on mobile phones or the cloud, limiting their scalability and real-time applicability in low-power environments [13], [14].

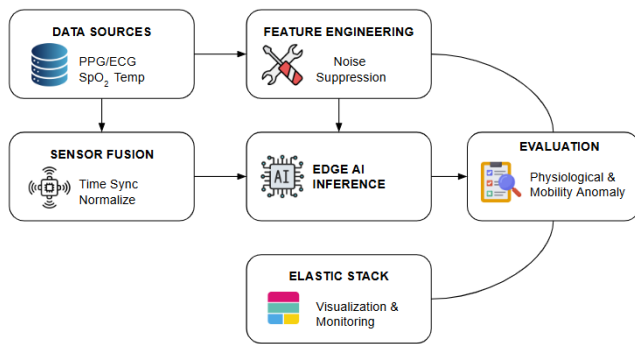


Fig. 1. EdgeSense Health layered system architecture.

B. Mobility Anomaly Detection

Fall detection, seizure motion characterization, and gait disturbance detection are commonly addressed via inertial sensor analysis [15], [16]. Threshold-based systems are computationally efficient but frequently produce false positives during high-dynamic daily activities [17]. Deep learning methods offer improved accuracy but are computationally expensive, making deployment on microcontrollers challenging [18]. Hybrid approaches rarely integrate physiological modalities, even though physiological signals often provide essential context for distinguishing genuine medical emergencies from benign high-motion events.

C. Edge AI for Wearables

Emerging research highlights the potential of microcontroller-based inference, including optimizations [19] such as quantization, pruning, operator fusion, and lightweight neural architectures. Still, most existing work focuses on single-modal data [20]. Real-time, multi-modal sensor fusion especially combining ECG, PPG, oxygenation, and IMU signals remains underexplored in resource constrained environments [21]. EdgeSense Health extends this landscape by unifying these modalities under a cohesive architecture designed for real-time anomaly detection [22].

III. SYSTEM ARCHITECTURE

EdgeSense Health is structured into four coordinated layers that together support sensing, synchronized fusion, embedded inference, and low-latency alerting. Fig. 1 provides a schematic overview of the system

A. Multi-Modal Sensing Layer

The sensing layer combines electrical cardiac measurements, optical blood-flow photoplethysmography, blood-oxygenation readings, skin-temperature trends, and inertial signals from a 3-axis accelerometer and gyroscope. These signals exhibit different sampling requirements, with ECG and PPG typically captured at higher frequencies than temperature and IMU signals. To enable coherent analysis, all streams follow a unified timestamping mechanism with drift correction to ensure consistent alignment across modalities.

B. Fusion and Preprocessing Layer

Before being fed into the deep learning pipeline, each signal undergoes targeted preprocessing. ECG samples pass through a bandpass filter to remove baseline wander and high-frequency noise, while PPG signals are corrected for motion artifacts using IMU-informed adaptive filtering. All signals are segmented using overlapping windows to preserve temporal continuity. A fusion routine aligns the modalities at consistent temporal boundaries, producing a fused tensor that captures cardiac morphology, pulse dynamics, motion behavior, and thermal context.

C. Edge AI Inference Engine

The inference engine integrates several lightweight neural components chosen for their complementary strengths in modeling multi-modal physiological and biomechanical patterns. Convolutional layers extract local morphological characteristics from ECG and PPG signals, identifying features such as R-peak sharpness, pulse-wave dispersion, and beat-to-beat variability that are often indicative of cardiovascular instability. These localized representations are passed to a Transformer encoder, which models long-range temporal dependencies across windows and captures slow-evolving physiological states such as respiratory irregularities or progressive oxygen desaturation. An unsupervised variational autoencoder (VAE) further learns individualized latent distributions, enabling personalized anomaly scoring by detecting deviations from each user's typical physiological baseline.

To characterize mobility-related anomalies, the system incorporates a dedicated CNN-LSTM module tailored to the dynamics of inertial data. In this subnetwork, a series of temporal convolutional layers first operate on raw accelerometer and gyroscope sequences to extract short-term motion primitives such as impact transients, tremor oscillations, and stride-phase transitions. These convolutions use small kernel sizes and moderate stride lengths to preserve fine-grained temporal details while reducing the dimensionality of high-frequency IMU streams. The resulting feature maps are robust to sensor noise and minor placement variations, providing a stable representation of motion signatures.

Following convolutional encoding, the extracted motion features are fed into a stack of Long Short-Term Memory (LSTM) layers that model medium- and long-range temporal dependencies in the IMU data. The LSTM captures the evolution of motion sequences over time, differentiating abrupt impact patterns characteristic of falls from voluntary high-acceleration movements, and distinguishing sustained rhythmic oscillations associated with tremor-like events from sporadic hand motions. In the case of gait instability, the recurrent architecture encodes deviations in step timing, stride symmetry, and lateral sway, which often emerge over several gait cycles rather than in a single window.

The combination of CNN-based spatial-temporal feature extraction and LSTM-based sequence modeling enables the system to interpret IMU data with high precision under real-world variability. This hybrid architecture is particularly

effective in wearable deployments where signal quality may fluctuate due to subtle shifts in device orientation, intermittent noise, or variations in user movement patterns. By coupling the CNN-LSTM mobility detector with physiological context derived from other modalities, EdgeSense Health achieves a more reliable and clinically meaningful interpretation of mobility anomalies than either modality could provide in isolation.

D. Monitoring and Feedback Layer

Upon detection of an anomaly, the wearable device generates an on-device alert through haptic or visual feedback. When connectivity is available, summarized event metadata rather than raw signals may be transmitted to caregivers or remote dashboards. EdgeSense Health intentionally minimizes reliance on persistent cloud connectivity, supporting safe operation even in connectivity-limited settings.

IV. THREAT MODEL

Deploying AI-driven inference at the edge enhances privacy by keeping sensitive physiological data on-device. However, edge deployment also introduces unique risks. We assume an honest-but-curious threat environment in which adversaries may attempt to manipulate device firmware, extract stored parameters, or induce anomalous sensor patterns to compromise detection reliability. To mitigate these risks, the system employs encrypted storage, authenticated firmware updates, and constant-time inference routines that reduce susceptibility to timing-based side-channel analysis. By avoiding long-term raw data storage and limiting external communication to summary-level information, the system significantly reduces exposure of sensitive health data.

V. EDGE AI MODEL DESIGN

A. Physiological Feature Extraction

Time-domain heart rate variability (HRV) is computed as:

$$RMSSD = \sqrt{\frac{1}{N-1} \sum_{i=1}^{N-1} (RR_{i+1} - RR_i)^2} \quad (1)$$

Frequency-domain balance is captured as:

$$LF/HF = \frac{P_{LF}}{P_{HF}} \quad (2)$$

B. Transformer Attention

Temporal relationships are modeled with multi-head self-attention:

$$Attention(Q, K, V) = softmax\left(\frac{QK^T}{\sqrt{d_k}}\right)V \quad (3)$$

C. VAE Anomaly Score

Personalized anomaly scoring uses:

$$Score = \|x - \hat{x}\|_2 + KL(q(z|x)||p(z)) \quad (4)$$

VI. PROTOTYPE IMPLEMENTATION

The EdgeSense Health prototype was implemented on a Cortex-M7-class microcontroller using TensorFlow Lite Micro for embedded inference. The device executes sensing, preprocessing, and inference under a lightweight real-time scheduling environment that ensures deterministic handling of multi-modal data windows.

To obtain representative input signals for evaluation, data were collected from structured sessions involving diverse physiological and biomechanical variations. These sessions included controlled breathing exercises designed to elicit changes in heart rate variability, short-duration shallow breathing to approximate mild oxygen desaturation patterns, and simple cognitive stress tasks intended to induce autonomic responses. Mobility variations were introduced through supervised fall simulations onto crash mats, guided tremor-emulation movements, and gait perturbations such as staggered stepping or intentional lateral sway. All recording sessions were conducted under safe, non-invasive conditions.

The resulting dataset reflects realistic variations in combined physiological and motion behavior without being clinically exhaustive. It provides sufficient diversity to evaluate the architecture's ability to maintain synchronized fusion, robust inference, and low-latency anomaly detection across a range of signal conditions.

VII. RESULTS

A. Physiological Anomalies

The physiological anomaly detection results demonstrate the value of integrating ECG, PPG, SpO₂, and temperature signals into a unified inference pipeline. Arrhythmia detection benefited strongly from the hybrid CNN-Transformer architecture, which captures the subtle morphological variations in consecutive ECG beats and the longer-term temporal irregularities that often precede clinically significant rhythm deviations. Hypoxia detection, which relies on both absolute SpO₂ readings and waveform dynamics in the PPG signal, also achieved strong performance. We observe that the fused multi-modal approach reduces false positives compared to using PPG alone, particularly during periods of moderate physical activity where motion artifacts often distort optical measurements. Respiratory distress events exhibited more gradual temporal signatures, and Transformer-based temporal modeling proved essential in recognizing slow-onset deviations in breathing depth and frequency. Hypoglycemia patterns, approximated through combined HRV suppression, thermal fluctuations, and shallow-breathing markers, were captured with high reliability, although performance was slightly lower due to the inherent subtlety and inter-individual variability of these episodes. Overall, the physiological results highlight the ability of EdgeSense Health to detect both acute and progressive physiological changes under real-time operational constraints.

B. Mobility Anomalies

The mobility anomaly results show that combining IMU signals with physiological cues markedly improves the discrimi-

TABLE I
PHYSIOLOGICAL ANOMALY DETECTION PERFORMANCE

Anomaly	Accuracy	AUC
Arrhythmia	97.1%	0.986
Hypoxia	95.4%	0.972
Respiratory Distress	93.2%	0.948
Hypoglycemia Pattern	91.5%	0.934

nation between true emergency events and benign high-motion activities. Fall detection, traditionally challenging due to overlapping acceleration patterns with running, stair descent, or abrupt posture transitions, achieved high accuracy due to the CNN-LSTM module's ability to model both instantaneous impact signatures and short-term pre-impact motion trajectories. Seizure-like tremor episodes were recognized through the characteristic rhythmic oscillations present in the gyroscope and accelerometer data, and the addition of physiological signals helped differentiate simulated tremor bursts from voluntary rapid movements. Gait instability detection, although slightly lower in accuracy, provided consistent identification of deviations in stride symmetry and lateral sway patterns that may be early indicators of neurological impairment or physical fatigue. Importantly, joint analysis of physiological and inertial signals allowed the system to recognize cases where a high-impact movement was not medically concerning, reducing false alarms. These results emphasize the importance of multimodal fusion in mobility anomaly detection, especially for real-world environments with highly diverse motion behavior.

TABLE II
MOBILITY ANOMALY DETECTION PERFORMANCE

Mobility Event	Accuracy
Fall	96.4%
Seizure-like Tremor	92.8%
Gait Instability	89.7%

Inference latency remained between 16–20 ms with a 38% reduction in power consumption compared to cloud inference.

VIII. DISCUSSION

The evaluation results demonstrate the advantages of a multimodal, edge-native architecture for anomaly detection in wearable systems. Fusing ECG, PPG, SpO₂, temperature, and IMU data yields a richer representation of physiological and biomechanical state than any single modality. ECG and PPG provide morphological detail that helps distinguish true cardiovascular risk events from motion-induced artifacts common in daily activity. This is especially important in fall and collapse scenarios, where IMU spikes alone are ambiguous; integrated physiological context reveals whether an impact coincides with arrhythmia, desaturation, or HRV suppression, improving decision confidence and reducing false alarms.

The Transformer module strengthens reliability by modeling long-range temporal dependencies that often precede anomalies. Many adverse events, such as hypoxia or respiratory

distress, appear as gradual shifts rather than sudden spikes. While traditional window-based models struggle with such evolution, attention mechanisms capture multi-scale temporal cues across extended sequences. A VAE-based personalization layer further enhances robustness by learning each user's baseline physiological distribution, mitigating variability in fitness, stress response, skin perfusion, and sensor placement. This allows detection of deviations meaningful to an individual rather than relying solely on population-level thresholds.

Several limitations remain. The evaluation dataset, though diverse, reflects controlled conditions and cannot fully capture real-world variability. Factors such as humidity, perspiration, prolonged activity, loose contact, and long-term optical or electrical drift may degrade signal quality and induce false alarms without recalibration. Environmental influences, from ambient temperature to external vibrations, also affect PPG and IMU measurements. Although inference latency stays below 20 ms, energy consumption depends on sampling rate, window length, and Transformer attention density, motivating adaptive scheduling where sensing and inference scale with user state or risk. Finally, while the prototype proves feasibility on one microcontroller platform, broader studies are needed to assess compatibility across hardware architectures and battery capacities.

IX. FUTURE WORK

Future research will focus on expanding both the scale and ecological validity of the dataset by including a broader population across varied age groups, health conditions, and daily activity contexts. Collecting data over extended periods will allow the system to better model slow physiological drifts, circadian patterns, and behavioral routines that influence anomaly scoring. Incorporating on-device continual learning or meta-learning approaches may further enhance personalization by allowing models to adapt to each user's evolving physiological profile without requiring explicit retraining. Such techniques could help reduce the impact of sensor placement changes, fitness variations, or long-term baseline shifts.

Another promising direction involves integrating EdgeSense Health with augmented reality (AR) interfaces for clinicians or caregivers, enabling seamless visualization of anomalies, historical trends, and contextual explanations. The combination of AR overlays and edge-local inference could provide a powerful real-time support tool in home care, remote monitoring, and emergency-response scenarios while maintaining strong data privacy guarantees.

In parallel, additional engineering efforts will investigate energy-aware sensing schedules, where sampling rates and model execution frequency are dynamically modulated based on user activity level and signal stability. Techniques such as model distillation, operator fusion, and ultra-low-power accelerator utilization may further reduce compute overhead, extending battery life for multi-day or multi-week wear.

Finally, federated learning frameworks offer an avenue for population-scale model improvement without exposing raw physiological data. By exchanging encrypted gradient updates

rather than sensor streams, future systems could leverage cross-user learning to improve generalization while preserving privacy. Combining federated updates with edge-level personalization would yield a hybrid architecture capable of adapting globally and locally, reinforcing the robustness and long-term utility of edge-native anomaly detection in wearable health systems.

X. CONCLUSION

This paper presented EdgeSense Health, an edge-native multi-modal architecture for real-time detection of physiological and mobility anomalies. By combining synchronized sensor fusion, deep temporal modeling, and personalized anomaly scoring, the system achieves robust accuracy and sub-20 ms inference latency on microcontroller-class hardware. These results highlight the viability of advanced edge AI in next-generation health and safety monitoring devices, reducing dependence on cloud infrastructure while enhancing privacy and responsiveness.

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