

Enhancement Of Medical Images Using Image Processing In Matlab

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Abstract: This paper gives the simple guideline to enhance the Medical images using MATLAB. Medical images are one of the fundamental images, because they are used in more sensitive field which is a medical field. The main goal of this study is to improve features and gain better characteristics of medical images for a right diagnosis. The proposed techniques start by the median filter for removing noise on images followed by unsharp mask filter which is type of sharpening. Medical images were usually poor quality especially in contrast. For solving this problem, we proposed Contrast Limited Adaptive Histogram Equalization (CLAHE) which is one of the techniques in a computer image processing domain, then for smoothing image data we used here Average (mean) filter thus eliminating noise.

Key words: Medical images, median filter, unsharp mask, contrast limited adaptive histogram equalization, average filter

INTRODUCTION :

Image enhancement:

In image enhancement, the goal is to accentuate certain image features for subsequent analysis or for image display. Examples include contrast and edge enhancement, pseudocoloring, noise filtering, sharpening and magnifying. Image enhancement is useful in feature extraction, image analysis and visual information display. The enhancement process itself does not increase the inherent information display in the data. It simply emphasizes certain specified image characteristics. Enhancement algorithms are generally interactive and application dependent. Image enhancement techniques such as contrast stretching map each grey level into another grey level by a pre-determined transformation. An example is the histogram-equalization method, where the input

levels are matched so that the output grey level distribution is uniform. This has been found to be a powerful method of enhancement of low contrast images. Other enhancement techniques perform local neighborhood operations as in convolution; transform operations as the discrete Fourier transforms [3]. It is an indispensable tool for researchers in a wide variety of fields including (but not limited to) medical imaging, art studies, forensics and atmospheric sciences. There are several techniques for enhancing digital images without spoiling it. The enhancement techniques can generally be classified into the following two classes:

- Spatial domain methods
- Frequency domain methods

In spatial domain methods, we directly deal with the pixels of image. The pixel values are manipulated to achieve coveted enhancement. In frequency domain techniques, the image is first transferred into frequency domain. It means that, the Fourier Transform of the image is computed first. All operations of image enhancement are executed on the Fourier transform of the image and then the Inverse Fourier transform is executed to obtain the resultant images. These enhancement operations are performed in order to modify the image brightness, contrast or the distribution of the grey levels. As a consequence the pixel value (intensities) of the output image will be modified according to the transformation function used in several domains where images should be analyzed and understood [1].

MATERIALS AND METHODS:

Overview:

There are a lot of techniques used in image enhancement or restoration including low pass filtering, high pass filtering, sobel edge filtering, median filtering, histogram equalization

and its various. Proposed method consists of three steps as following:

- Median filter for noise reduction
- UnSharp Mask filter (USM) for edges sharpening
- Contrast Limited Adaptive Histogram Equalization (CLAHE) for contrast enhancement [1,8]
- Average (mean) filter for smooth data [2,8]

Median filter for noise reduction:

Filtering is a part of image enhancement which is used to enhance certain details such as edges in the image that are relevant to the application. In addition to that, filtering can also be used to eliminate unwanted elements of noise. Medical images usually contain salt and pepper noise. This noise appears due to the presence of minute gray scale variations in the image. Median filtering is a popular technique of the image enhancement for removing impulse noise without effectively reducing the image sharpness [1]. The median filter is a non-linear digital filtering technique, frequently used to remove noise from images. It is mostly useful to reduce speckle noise and salt and pepper noise. Its edge-preserving nature makes it practical in cases where edge blurring is undesirable. The median filter is defined as follows: To compute the output of a median filter, an odd number of sample values are ranked, and the median value is used as the filter output. It is reasonable to assume that the signal is of finite length, consisting of samples from $X(0)$ to $X(L-1)$. If the filter's window length is $N=2k+1$, the filtering procedure is given by:

$$Y(n) = \text{med}[X(n-k), \dots, X(n), \dots, X(n+k)]$$

Where $X(n)$ and $Y(n)$ are the input and the output sequences, respectively. This is the non recursive Median filter. It has been first shown that any sequence of length L is converted under repeated median filtering to the root signal after at most $(L-2)/2$ passes [2, 8].

Unsharp mask filter for edges sharpening:

Unsharp filtering is an uncomplicated sharpening process that gains its name from the study which it improves edges and other high frequency components in images through a process that deducts a smoothed or unsharp version of

images from the input images. In our study, the use of the classical unsharp mask filter after median filter to reduce the remained noise and sharpen the edges. Firstly it is obtained a blurred form of the original image. This is carried out by applying the low-pass filter, in our case Gaussian blur algorithm using a small radius. We used a two pixel radius and applied Gaussian blur filter only two times. The blurred form of the image is then pixel deducted from the original image and so it is obtained the high pass component. The output image is obtained by adding the high-pass component to the original image. Because the output image could contain also pixels with negative values, it is then normalized. No threshold cutoff was used. The two steps for the unsharp mask filter are mentioned below:

- Unsharp mask filter creates edge images $g(x,y)$ from input images $f(x,y)$ in this Eq. 1.

$$g(x,y) = f(x,y) - f_{\text{smooth}}(x,y) \quad (1)$$

Where, $f_{\text{smooth}}(x,y)$ is a smoothed form of $f(x,y)$ (Gaussian blur algorithm) as shown in Fig. 1.

- The edge images from the result of subtracting input images from low pass signal could be utilized for images sharpening by adding it backward into the input signal, as illustrated in Fig. 2. This function is represented as follows: $f_{\text{sharp}}(x,y) = f(x,y) + k * g(x,y)$ (2)

Where, k is a scaling constant, values for k ($k \geq 0$), for generally. When $k > 1$, the process is referred to as Highboost filtering. In our process, we have applied $k=1$.

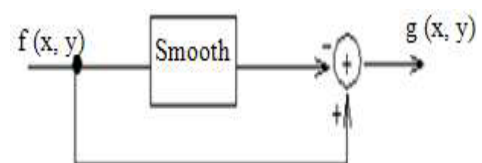


Fig. 1: Spatial sharpening

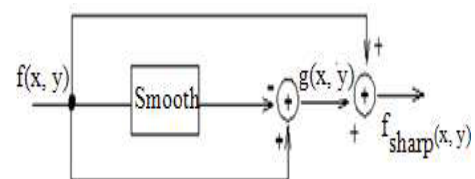


Fig. 2: The complete unsharp filtering operator

The basic advantage of the unsharp filtering over other sharpening filters is the control flexibility, because a vast majority of other sharpening filters do not supply any user-adjustable parameters. Unsharp filtering as other filters enhances fine detail and edges in digital images [1].

Contrast Limited Adaptive Histogram Equalization (CLAHE):

Contrast limited adaptive histogram is a technique utilized for improving the local contrast of images. It is a generalization of ordinary histogram equalization and adaptive histogram equalization. CLAHE does not operate on the whole image works like ordinary Histogram Equalization (HE), but it works on small areas in images, named tiles. Problems associated with HE and AHE can be limited by reducing contrast enhancement particularly in homogeneous areas. The algorithm (Contrast Limited Adaptive Histogram Equalization (CLAHE)) limits the slope associated with the gray level assignment scheme to prevent saturation. This process is accomplished by allowing only a maximum number of pixels in each of the bins associated with the local histograms. After "clipping" the histogram, the clipped pixels are equally redistributed over the whole histogram to keep the total histogram count identical.

The CLAHE method can be divided into steps to achieve as following:

- The Medical image is divided into contextual regions which are continuous and non-overlapping. Each contextual region size is $M \times N$ (the contextual regions size was set here to 8×8)
- The histograms of each contextual regions are calculated
- The histograms of each contextual regions are clipped (A clip limit was set here to 0.01) The pixels number in the contextual region is equally distributed to each gray level. Then the average number of pixels in each gray level is defined as follows:

$$N_{av} = \frac{N_{cr-x} \times N_{cr-y}}{N_g} \quad (3)$$

Where,

N_{av} = Average number of pixels

N_g = Gray levels number in the contextual region

N_{cr-x} = Pixels number in the x dimension of the contextual region

N_{cr-y} = pixels number in the y dimension of the contextual region

Based on the Eq. 3, the N_{av} can be calculated by the eq. 4:

$$N_{ac} = N_{cr-x} \times N_{cr-y} \quad (4)$$

Where, N_{ac} is actual clip-limit; N_{ci} is the maximum multiple of average pixels in each gray level of the contextual region. The original and clipped histograms are shown in Fig. 3. In Fig. 3(a) if the number of pixels is greater than N_{ci} , the pixels will be clipped. The total number of clipped pixels is defined as $N_{\Sigma c}$, and then the number of pixels distributed averagely into each gray level is given by Eq. 5:

$$N_{acis} = \frac{N_{\Sigma c}}{N_g} \quad (5)$$

After the above distribution, the remaining number of clipped pixels is expressed as LP_N and then the step of distributed pixels is given by

$$Pd = \frac{N_g}{N_{lp}} \quad (6)$$

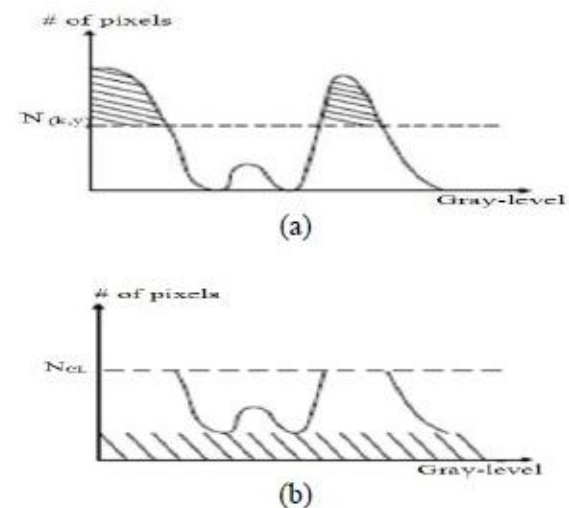


Fig. 3: Original and clipped histograms (a): original histogram (b): clipped histogram [1]

Average Filter:

The Average (mean) filter smooth image data, thus eliminating noise. This filter performs spatial filtering on each individual pixel in an image using

the grey level values in a square or rectangular window surrounding each pixel[2].

For Example:

$$\begin{bmatrix} a1 & a2 & a3 \\ a4 & a5 & a6 \\ a7 & a8 & a9 \end{bmatrix} \text{ 3x3 filter window}$$

The Average filter computes the sum of all pixels in the filter window and then divides the sum by the number of pixels in the filter window:

$$\text{Filtered pixel} = \frac{\sum (a1 + a2 + a3 + a4 + \dots + a9)}{9}$$

Average filter method is also called neighborhood average method. The essential idea of this method is to replace gray scale value of the center pixel by average value of neighborhood pixel gray scale. Its filter features are analyzed as follows: Suppose the noise model is

$$g(i, j) = f(i, j) + n(i, j) \quad (7)$$

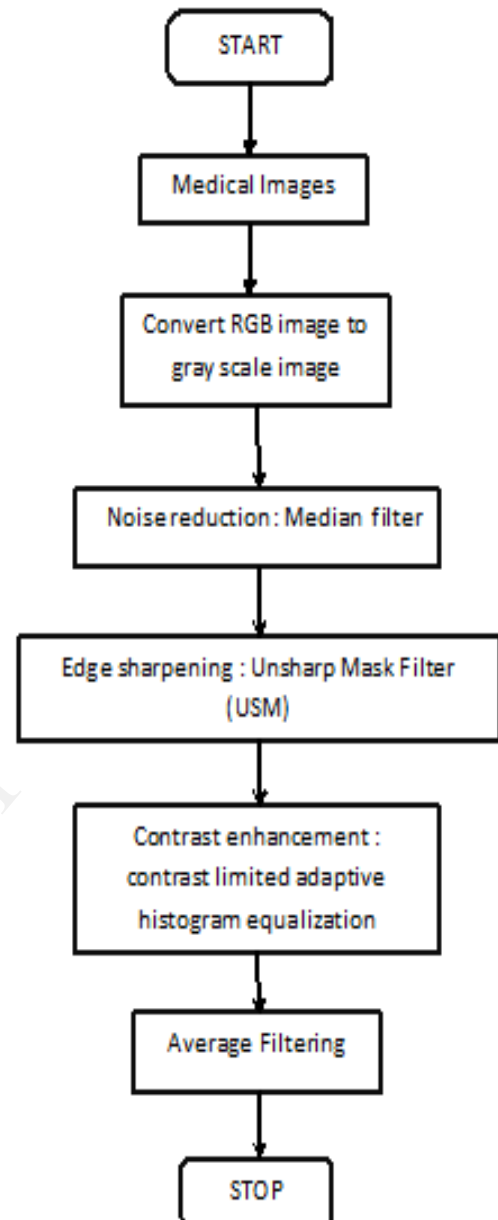
The image after neighborhood smoothing is

$$g(i, j) = \frac{1}{M} \sum_{(i, j) \in S} g(i, j)$$

$$= \frac{1}{M} \sum_{(i, j) \in S} f(i, j) + \frac{1}{M} \sum_{(i, j) \in S} n(i, j)$$

..... (8)

FLOWCHART:



Flowchart describes the image enhancement process using filtering techniques, histogram equalization. Median, Average and Unsharp mask filtering techniques are used to enhance the image in terms of improving the visual aspect of images.

In the first step, the original medical image is taken which is in the form of RGB image which is 3D image. In the second step, we are converting RGB image to Gray scale image which is 2D image. In the third step, it can be filtered using median filtering which is used for noise reduction. In the fourth step, it can be improved using unsharp

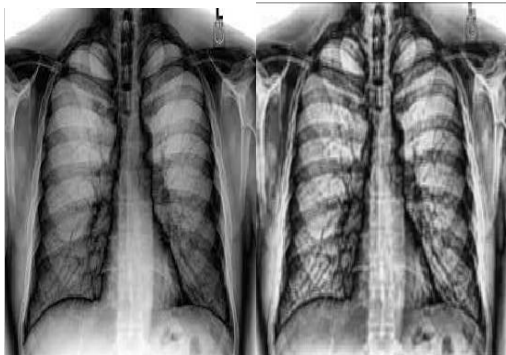
mask filtering it is used for edge sharpening of the image.

In the fifth step, it can be improved using contrast enhancement technique specially we are used contrast limited adaptive histogram equalization (CLAHE) . Thereafter, the Average filtering technique is applied for smoothing image data, then the output image is generated. The enhanced images improvement from the original images depends on medical images modalities.

RESULTS:

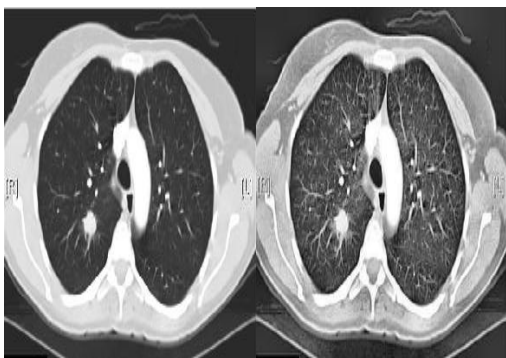
The proposed methods have applied on different partsof the body. Some results are illustrated below[8]:

Fig.4: CT image



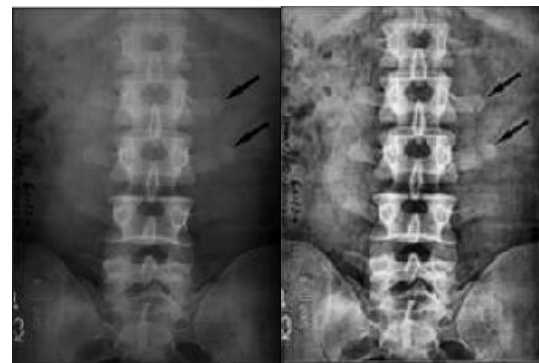
(a) (b)

Fig.5: CT image



(a) (b)

Fig.6: X-RAY image



(a) (b)

Fig.7: MRI image



(a) (b)

Fig.8: Angiogram image



(a) (b)

Fig.9:CT image

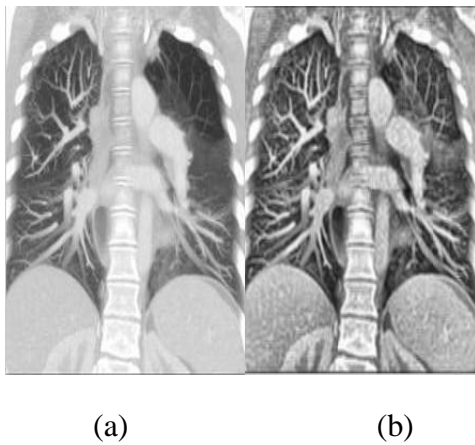
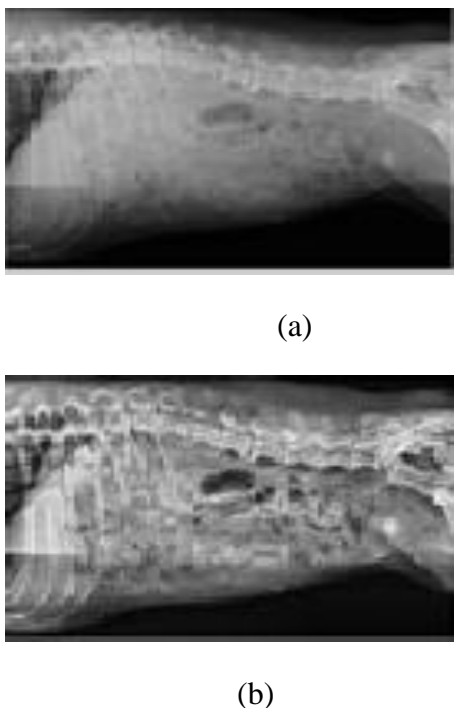


Fig.10: X-RAY image



where ,(a) Original images (b) resultant images after applying proposed method

CONCLUSION:

In the proposed method, we have enhanced medical images by effective enhancement algorithms which are median filter, unsharp mask filter, contrast limited adaptive histogram

equalization and average filter. The proposed methods have been implemented by MATLAB .

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