Abstract—Blood cancer is a form of cancer which attacks the
blood, bone marrow, or lymphatic system. It is diagnosed with a
blood test in which specific types of blood cells are counted by
hematologist. We considered only acute myelogenous leukemia
which is one of the blood cancer type which categories under
acute leukemia and mostly comes among adults. Need for
automatic diagnosis of leukemia arises when doctors recognize
cancers under a microscope which has complete manual work
and it’s not good for the patient. Automatic diagnosis system
which helps hematologists for easier identification and early
detection of leukemia from blood microscopic images which will
improve the chances of survival for the patient. In this proposed
system, which mainly composed of four main stages are
preprocess stage, segmentation stage, feature extraction stage
and classification stage respectively. This system framework
consists simple and known technique such as K-means clustering,
Local Directional path (LDP), and support vector machine
(SVM) respectively. The condition of a patient is shown as
normal or abnormal status with the help of classifier. The overall
system performance is evaluated using the defined parameters
such as sensitivity, specificity, f-measure, and precision
whichhused for calculating the accuracy. Ninety microscopic blood
images were tested, and the proposed framework managed to
obtain 98% accuracy. Finally, we compare the results of some of
the existing systems with our proposed system to show our
achievement on accuracy.

Keywords—Acute myelogenous leukemia, Pre-processing
stage, feature extraction stage, classification stage and
segmentation

I. INTRODUCTION

The term leukemia comes from the Greek word "leukos"
meaning "white" and "aim" meaning "blood." It refers to the
cancer of the blood or the bone marrow (where blood cells are
produced). The Leukocytes which play a major role in the
diagnosis of different diseases. The Extracting information
from WBC is valuable for hematologists as in [1]. Diagnosing
leukemia is based on the fact that white cell count are
increased with immature blast cells (lymphoid or myeloid),
and neutrophils and platelets are decreased as in [2], [3].
Therefore, hematologists routinely examine blood smears
under microscope for proper identification and classification
of blast cells. The presence of the excess number of blast cells
in peripheral blood is a significant symptom of leukemia.

There are four main types of leukemia: acute
lymphoblastic leukemia (ALL), acute myeloid leukemia
(AML), chronic lymphocytic leukemia (CLL) and chronic
myeloid leukemia (CML), as well as a number of less
common types. ALL is the most common type of leukemia in
young children. CLL most often affects adults over the age of
55. AML occurs more commonly in adults than in children,
and more commonly in men than women. AML is treated with
chemotherapy. CML occurs mainly in adults; a very small
number of children also develop this disease. Fig. 1 shows
examples of leukemic cell images gathered from the web
source [4].

Fig. 1. Examples of leukemic blood cells showing the four different types of
leukemia: (a) ALL, (b) AML, (c) CLL, and (d) CML.

AML is confirmed when the marrow contains more than
30% blasts as in [2]. AML is a fast-growing cancer of the
blood and bone marrow. It is fatal, if left untreated, due to its
rapid spread into the bloodstream and other vital organs as in
[5]. Early diagnosis of the disease is a fundamental to the
recovery of patients, particularly in the case of children as in
[5]. If the described symptoms are present, blood tests, such as
a full blood count, renal function and electrolytes, and liver
enzyme and blood count, have to be done as in [5]. Since there
is no staging for AML, choosing the type of treatment can
vary from chemotherapy, radiation therapy, bone marrow
transplant, and biological therapy as in [6]. The Input image
which is accessed from the American Society of Hematology
(ASH) online image bank of leukemia cells from the web
source [7]. The Fig. 2 shows two different input images, one
depicting healthy cells from non-AML patients and others
from AML patients.

This paper is structured as follows. Section II focuses in
detail on different literature reviews. Section III shows the
design methodologies being used to perform segmentation,
feature extraction, and classification. The Section IV gives detailed computer simulation process with the result for different datasets of input images. The Section V contains conclusions and future work.

Fig. 2. Input Microscopy Images. (a) Myeloblasts from AML patients. (b) Healthy cells from non-AML patients.

II. PREVIOUS WORK

A number of research efforts for segmentation have been reported in the last few years. In the past, digital image processing techniques have helped to analyze the cells that lead to more accurate, standard, and remote disease diagnosis systems. However, there are a few complications in extracting the data from WBCs due to wide variation of cells in shape, size, edge, and position [1]. A detailed survey of the existing methods can be found in [2], [5], [6], [8]-[14], [16], [18], [20] and [24]-[26] and can be classified mainly into three main categories are segmentations, Features extraction and classifications.

In Medical diagnosis process one of the most important step is to segment the nucleuses from cluster of nucleus. A watershed segmentation algorithm to segment nucleus from the surrounding cytoplasm of cervical cancer images. When it comes to peripheral blood or bone marrow smears, region-based or edge-based schemes as in [8]. The merging technique for Nuclei Segmentation as in [9]. The work in [10], [11], [15] and [13] presented an unsupervised color segmentation to bring out the WBCs from acute leukemia images. The color image segmentation algorithms, it was concluded that color images present more reliable image segmentations than gray-level images which gives better segmentation but it has over-segmentation problem. The selective filtering to segment leukocytes from the other blood components and classification accuracy obtained was 95% for a different set of similar blood images using k-mean clustering as in [13]. The contour signature to identify the irregularities in the nucleus boundary with better accuracy as shown in [12].

For Feature extraction in image processing is a technique of redefining a large set of redundant data into a set of features of reduced dimension. Transforming the input data into the set of features is called feature extraction. A more robust facial and texture descriptor, named as Local Directional Pattern (LDP), was devised, where the LDP representation of face demonstrated better recognition performance than LBP as in [14]. Mostly, Local Binary Pattern (LBP) and its variants, as a feature descriptor for facial expression representation and it uses the information of intensity changes around pixels as in [19]. The Local Directional Pattern (LDP) principle which features has overcome the limitations of LBP features as in [14], [19], and [21]. However, LDP is derived from the edge responses which are less sensitive to illumination changes and noises. The performance of LDP representation is evaluated with two machine learning methods: Template matching and Support Vector Machines (SVM) with different kernels. Here we going to use SVM which is a supervised classifier.

For Image classifier is used in medical diagnosis process for increase the accuracy on effected nuclei detection and segmentation. The surveyed for Cell Phase Identification using KNN classifier and Nuclei Tracking using matching process as in [9]. So this shows that, it produces the 94% accuracy of nuclei detection and tracking algorithm achieved more than 90% tracking accuracy. But Errors happen over segmentation problem when daughter cell nuclei overlap with nearby nuclei right after division and need to and improve the segmentation process. With the SVM classifier with 92% accuracy achievement as in [18].

In this Project, only Acute Myelogenous Leukemia (AML) is considered. This technique greatly depends on the operator’s ability and fatigue levels. The most Common drawback observed from various survey from different literature and many more which as a problem of over-segmentation of cluster of nucleus and accuracy of detection of affected nuclei problems. The problem of images with high degree of cell overlapping has overcome as in [18] with help of SVM classifier. Thus, the main goal of our paper is to implement a fully automated classifier system for AML and to increase the accuracy of finding exact effected cells and overcome the over-segmentation of cluster of nucleus problem which influence our goal.

III. SYSTEM METHODOLOGY

In this Section, the framework for the proposed segmentation method is described. The flow diagram of the proposed method is shown in Fig. 3 which consists of four stages: Pre-processing stage, Segmentation stage, feature extraction stage and Classification stage respectively. The details of the framework are given in the following subsections:

A. Image Pre-Processing Stage

In this stage, input image is obtained and image is resized as needed for further process. The resized image which is RGB color space converted into Gray scale level image. Finally, then the selective median filtering applied which used to remove unwanted effects such as noise from the image.
B. Image segmentation stage

In this stage, goal of image segmentation is to extract important information from an input image. It plays a key role since the efficiency of subsequent feature extraction and classification relies greatly on the correct identification of the myeloblasts. The Image segmentation has developed for gray-level images. Segmentation in this system is performed for extracting the nuclei of the leukocytes using K-mean clustering. K-means is still widely used as in [1], [13]. In this paper, we chose clusters corresponding to only intensity information. Images of this sort, also known as black-and-white, are composed exclusively of shades of gray, varying from black at the weakest intensity (background) to white at the strongest intensity (nucleus). Here, every pixel is assigned to one of these classes using the properties of the cluster center.

C. Image Feature Extraction stage

Feature extraction in image processing is a technique of redefining a large set of redundant data into a set of features of reduced dimension. Transforming the input data into the set of features is called feature extraction. Feature selection greatly influences the classifier performance; therefore, a correct choice of features is a very crucial step as in [17]. We implemented these features on whole images in our system. Those features were considered to boost the classifier performance.

Local Directional Pattern (LDP): LDP is a gray-scale texture pattern which characterizes the spatial structure of a local image texture. A LDP operator computes the edge response values in all eight directions at each pixel position and generates a code from the relative strength magnitude. Since the edge responses are more illumination and noise insensitive than intensity values, the resultant LDP feature describes the local primitives including different types of curves, corners, and junctions, more stably and retains more information. LDP operator use the edge response values of neighborhood pixels and encode the image texture. The LDP is computed as in [14].

The LDP assigns neighbor pixel, N as 8 bit binary code to each center pixel of an input image with window size, n as 1 and k=3 as 3x3 matrix. The Features information is extracted by histogram plot. To construct a histogram, the first step is to find Nbin value which is the range of values, i.e., that is, divide the entire range of values into a series of small intervals and then count how many values fall into each interval using (1).

\[ N_{\text{bin}} = \frac{N!}{k! \cdot (N-n)!} \]  

(1)

The histogram is constructed by the number of occurrences of each pixel value and minimum and maximum pixel range. Then variation between normal and abnormal is predicted easily on histogram plot.

D. Image classification stage

The selection of a classification technique for classification is a challenging problem because an appropriate choice given the available data can significantly help improving the accuracy in credit scoring practice as in [1], [2]. There is a plenty of statistical techniques, which aim at solving binary classification tasks. In this project, we use a support vector machine (SVM) for constructing a decision surface in the feature space that bisects the two categories, i.e., cancerous and noncancerous, and maximizes the margin of separation between two classes of points. SVMs are a promising nonlinear nonparametric classification technique, which already showed good results in the medical diagnostics, optical character recognition, electric load forecasting, and other fields as discussed on [20], [23].

An SVM is primarily a two-class classifier. It can be either linear or nonlinear. In this paper, we choose a linear SVM two-class classifier; because it is not computationally expensive, it does not employ the kernel trick explicitly and it achieves, in general, a good performance as in [20], [23] and [26]. The classification using the SVM, a statistical method called cross-validation is used for evaluating and comparing learning algorithms. Cross-validation is a technique for judging how the results of a statistical analysis will generalize to an independent data set. It is mainly used in settings where the goal is prediction and where one wants to estimate how precisely a predictive model will perform in practice. Three kinds of validation techniques have been used: K-fold, holdout, and leave-one-out as in [1], [2]. A quantitative analysis of the performance of the proposed method for segmentation is carried out in terms of accuracy. The accuracy is calculated from a dataset of sample images which are tested individually.

The SVM Classifier gets the normalized value of the histogram from feature extraction stage and then SVM is trained with obtained histogram features. A collection of each sample image is tested. Then these tested image relate to the possible outcomes of the classifier system. When attempting to classify a specimen, there are four possibilities: True Positives (TP), when cancer cells are correctly identified; False Positives (FP), when non-cancer cells are identified as cancerous; True Negatives (TN), when non-cancerous cells are correctly identified; and False Negatives (FN), when cancer cells are identified as noncancerous as in [2]. Here, we classified as normal or abnormal conditional of the microscopy input image sample. These parameters are calculated, the overall accuracy of tested Image which is formulated as mentioned as shown in Table I given in [2], that higher values of these parameters will lead to better accuracy.

![Table I. Parameter for Performance Evaluation](attachment:image)

\[ \text{Precision} = \frac{TP}{TP + FP} \]
\[ \text{Specificity} = \frac{TN}{TN + FP} \]
\[ \text{Sensitivity} = \frac{TP}{TP + FN} \]
\[ \text{F-measure} = \frac{2 \cdot \text{Precision} \cdot \text{Sensitivity}}{\text{Precision} + \text{Sensitivity}} \]
\[ \text{Accuracy} = \frac{TP + TN}{TP + TN + FP + FN} \]
IV. COMPUTER SIMULATION RESULTS

The proposed technique has been applied on peripheral blood smear images obtained from diagnosis center, as aforementioned. A microscopic blood image of any size is considered for evaluation. The superiority of the scheme is demonstrated with the help of some sample of inputs. In this project, we can use MATLAB 7.5 and above version for analysis of diagnosis samples.

Pre-Processing Stage: Using MATLAB software, get the input blood sample image from data sample set. Let be, input image, Obtained Image is processed by gray scale conversion to get intensity information and then if any noise, then gray level image apply to median filter as shown in Fig. 4 (a)-(f),

![Input sample image](image1)
![Converted Gray scale image](image2)
![Filtered Gray scale image](image3)

Fig. 4. (a), (d) Input sample image. (b), (e) Converted Gray scale image and (c), (f) Filtered Gray scale image.

Image Segmentation Stage: Result obtained from Pre-processing stage will provide Gray level Intensity information of image for easier segmentation of WBC Nucleus from cluster of nuclei. This image segmentation done by using k-mean Clustering technique. This k-mean Clustering Technique to group your objects based on features into K number of group. The grouping is done by minimizing the sum of squares of distances between data and the corresponding cluster centroid. Thus, the purpose of K-mean clustering is to classify the data. The Clusters of objects (k=4) for input image is shown in Fig. 5 for input image of Fig. 2 (a) and (b). Now, segmented image output for Fig. 2 (a) and (b) is shown in Fig. 6 (a) and (b).

![Segmented image](image4)
![Segmented image](image5)

Fig. 5. Clustered of object for Fig. 2 (a) and (b). (a) 1st Cluster, (b) 2nd Cluster, (c) 3rd Cluster and (d) 4th Cluster

![Segmented image](image6)
![Segmented image](image7)

Fig. 6. (a) Final Nuclei Segmented Output image for Fig. 2 (a). (b) Final Nuclei Segmented Output image for Fig. 2 (b).

Image feature extraction stage: Nuclei is segmented from the previous stage and then LDP operator is applied for extracting features of segmented nuclei. Fig. 7 shows the texture analysis of LDP for Fig. 6 which as segmented image. The features of segmented image are obtained by constructing a histogram plot. To construct histogram, we have calculated the Number of bins value. Thus, small variation of number of count values in each pixels is used to differentiate normal or abnormal case. The histogram plots of both normal and abnormal is shown in Fig. 8.

![Segmented image](image8)
![Segmented image](image9)

Fig. 7. LDP based Texture analysis of (a) nuclei segmented image of Fig. 6 (a) and (b) nuclei segmented image of Fig. 6 (b).

![Histogram](image10)
![Histogram](image11)

Fig. 8. Histogram plot for (a) Fig. 7 (a) and (b) Fig. 7 (b).

Image classification stage: The values of Histogram will be very high in range of thousands and this high range value can’t be implemented in SVM classifier directly. So that normalized values are calculated and applied to SVM classifier. SVM is used to differentiate two status of patient i.e., whether Abnormal or Normal case for given blood sample under test. The proposed system result shows dialog box as normal or abnormal condition of patient. In Abnormal case, as mentioned earlier, larger number of WBC (cluster of Blue Nuclei-WBC) leads to the Leukemia cancer which shows abnormally of patient as shown in Fig. 9 (a) and large variations in number of count of each pixels of abnormal case as shown in Fig. 8 (a). Whereas, in Normal case, Count of WBC (Blue Nuclei) will less which shows patient does not has cancer which is shown in Fig. 9 (b) and small or no variations in number of count of each pixels of normal case as shown in Fig. 8 (b). The performance evaluation is calculated using the parameter values shown in Table II form tested images. The
Overall accuracy of our system compared with few existing system is shown in Fig. 10.

Fig. 9. (a) Abnormal condition and its Status. (b) Normal condition and its Status.

Fig. 10. Overall accuracy of our system compared with few existing system.

<table>
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<tr>
<th>Parameters</th>
<th>Values</th>
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**TABLE II. PERFORMANCE EVALUATION TABLE**

V. CONCLUSION

This proposed system has been successfully the implemented and evaluated for an automated screening system for AML in blood microscopic images. It uses 90 high-quality 184 x 138 size images obtained from the American Society of Hematology, which has to be tested for leukemia. A feature set exploiting the texture factor of a blood cell image to get all the information required using histogram to do efficient classification. The impact of the LDP operator on the segmented image provided a promising feature for this analysis. Thus, 88 out of 90 images yields correct results of 98%, which shows the accuracy of tested images of the proposed system and presents a good demarcation between cancer and non-cancer status of a patient under test.

Further, research will focus on the collection of more samples to yield better performance and building an overall system for cancer classification. Then in future this diagnostic method can be tested for various diseases such as Ebola, Tumor, Brain cancer, etc.

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